

Creation of a New Bioartificial Myocardium: Dream or Reality?

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Ischemic myocardial disease, the main cause of heart failure, is a major public health and economic problem. Given the aging population, heart failure is becoming a bigger clinical issue and bigger financial burden (1, 2). Thus, research in heart failure is of relevant interest and importance, involving specialities as cellular and molecular biology, tissue engineering, genetics, biophysics and electrophysiology.

CELLULAR CARDIOMYOPLASTY

Follow up of congestive heart failure patients has mobilized a growing number of research teams over the past years. In the development of new therapies for heart failure, one of the most innovative procedures consists in the transplantation of stem cells into the myocardium for heart muscle regeneration. This approach is called “cellular cardiomyoplasty” (3, 4). Adult myocardium cannot effectively repair after infarction due to the limited number of stem cells. Thus, most of the injury is irreversible (5). For this reason, cell transplantation strategies for heart failure have been designed to replace damaged cells with cells that can perform cardiac work, either in ischemic or non-ischemic cardiomyopathies.

Grafting of healthy cells into the diseased myocardium holds enormous potential as an approach to cardiovascular pathology. The goal of cell transplantation is to grow of new muscle fibers (myogenesis) and/or to develop angiogenesis in the damaged myocardium that potentially may contribute to improve systolic and diastolic ventricular functions, and to reverse the postischemic remodeling process of the ventricular chambers (5).

The encouraging results of experimental studies (6-11) have opened the way to the clinical application of cellular cardiomyoplasty in patients with akinetic and non-viable post-infarction scar and low ejection fraction and in patients presenting idiopathic and chagasic cardiomyopathies (12-15). Cultured autologous cells do not raise immunological, ethical, tumorigenesis or donor availability problems. Thus, the development of cell therapy for heart failure is progressing according to a rigorous scientific methodology, from observation to experimentation to a careful evaluation of preliminary clinical results.

Current possibilities in cell therapy for myocardial regeneration are the transplantation into the damaged myocardium of different types of stem cells as: autologous myoblasts (originating from a skeletal muscle biopsy) (16), bone marrow stem cells (17), peripheral blood stem cells (18), vascular endothelial cells (19), mesothelial cells (removed from a biopsy of the omentum) (20), adipose tissue stem cells (21), and embryonic pluripotent cells (22).

Tissue engineering using biological and synthetic matrix can be associated with cell therapy, the goal is to develop a bioartificial myocardium (23-29). After several years of basic and surgical research, the MAGNUM Clinical Trial (Myocardial Assistance by Grafting a New Upgraded bioartificial Myocardium) was initiated by our group (30).

DEVELOPMENT OF BIOARTIFICIAL MYOCARDIUM

The objective of cellular cardiomyoplasty is to regenerate the myocardium by the implantation of living cells. However, in ischemic disease the extracellular matrix is often disrupted or destroyed. Therefore it could be important to associate a procedure aiming at regenerating both myocardial cells and the extracellular matrix. We are currently working to evaluate the potential of a biodegradable tridimensional matrix seeded with stem cells and grafted onto the infarcted ventricle (23).

Shortly after myocardial infarction, inflammatory cells such as neutrophils, monocytes and macrophages infiltrate the infarcted zone, and then the necrotic myocytes in the injured myocardium are replaced by collagen fibers. This process uniformly occurs in the whole infarcted area, and determines the degree of early infarct expansion. Prevention of the dilation, secondary to LV remodelling, can increase cardiac performance (5).

There are two types of collagen fibers in the normal adult heart, types I and III, produced by fibroblasts and myofibroblasts. The fiber type I represents 80% of collagen protein in the heart, and type III is near to 10%. These fibers provide structural support and give the heart properties that include stiffness and resistance to deformation, they have also shown an important role as a link between contractile elements of adjacent myocytes, carrying some information useful for cell function. In the infarcted zone the extracellular myocardial matrix is modified, collagen type I decreases from 80 to 40%. After experimental studies (23), a clinical trial was initiated by our group in ischemic patients using autologous bone marrow cell implanted into the infarct scars associated with the surgical implantation onto the epicardium of a cell-seeded collagen type I matrix.

Preliminary results showed that this procedure prevented myocardial wall thinning and limited postischemic remodelling (30).

PERSPECTIVES

Cell transplantation is becoming recognized as a viable strategy to improve myocardial viability and limit infarct growth. The major challenges for future research programs are the pre-conditioning for pre-differentiation of stem cells before transplantation, the optimization of the rate of surviving cells after myocardial implantation associating angiogenic therapy with myogenic cells, and the improvement of percutaneous cell-delivery procedures (31).

The development of a bio-artificial myocardium is a new challenge, in this approach tissue engineered procedures (26-28) are associated with cell-based myocardial regeneration. The MAGNUM Clinical Trial (Myocardial Assistance by Grafting a New Upgraded bioartificial Myocardium) have been initiated by our group (30, 32). Electrostimulation associated with cellular cardiomyoplasty was proposed by our group to transform passive cell therapy into “dynamic cellular support”. In protocols using bioengineered cell-seeded collagen matrix, electrostimulation may induce the differentiation and contraction of the grafted tissue (33, 34).

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